

# Biventricular Cardiac Model

This example demonstrates how to simulate a cardiac contraction on a simplified heart geometry, where only the ventricles are considered and the stimulus starts from the atrioventricular node.

During the cardiac cycle (heartbeat) an electrical stimulus generated from the sino-atrial node propagates throughout the entire heart. When excited, cardiac cells are subjected to an electric potential jump across their membranes. The transport and accumulation of ions and additional chemical reactions cause cells to contract. At a macro-scale these chemical and electrical processes trigger the contraction of the muscle tissue, the myocardium, allowing blood to be pumped to the arteries.

The muscle tissue (myocardium) is mainly composed of myocardial cells grouped in layered sheets that are aligned in a preferential direction (fibers). The fiber orientation strongly affects the mechanical and electrical tissue properties. This arrangement suggests that the cardiac tissue can be modeled as an anisotropic hyperelastic material.

The time and spatial evolution of the electric potential is described by the Aliev-Panfilov equations with a nonlinear current-voltage relation. This electrochemical model describes the quick rise of the cell's transmembrane electric potential (depolarization) and the return to its resting value (repolarization).

The tissue contraction in the hyperelastic model is obtained using an additive decomposition of the stress tensor. The actual contraction at cellular level is taken into account by introducing an additional stress (active stress) in the Solid Mechanics interface. This additional stress is voltage-dependent, and its evolution is described by additional partial differential equations.

The simplified heart geometry shown in Figure 1 includes the two elliptical ventricular chambers. The atria are not considered.

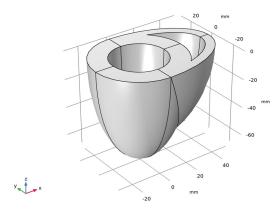


Figure 1: Geometry of the two ventricular chambers of the heart.

The base is located at Z = 0, and the left ventricle apex is located at Z = -70 mm. The ventricle dimensions are taken from Ref. 2 and shown in Table 1.

TABLE I: LEFT AND RIGHT VENTRICLE DIMENSIONS.

Geometry	Left ventricle	Right ventricle
x-semiaxis (epicardium)	30[mm]	51[mm]
y-semiaxis (epicardium)	30[mm]	30[mm]
z-semiaxis (epicardium)	70[mm]	60[mm]
Thickness	12[mm]	6[mm]

The ventricular wall (myocardium) is surrounded by the epicardium on the outside (Figure 2) and by the endocardium on the inside (Figure 3). These are not included in the model, but these terms will refer to the walls boundaries that are in contact with the myocardium.

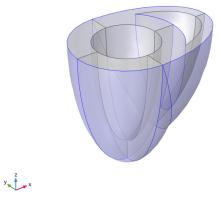


Figure 2: Boundaries in contact with the epicardium.

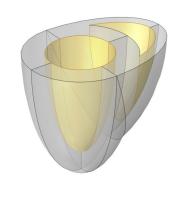


Figure 3: Boundaries in contact with the endocardium.

## FIBER DIRECTION

The fibers have an inclination of  $60^\circ$  at the endocardium ( $\theta_{\rm end}^{\rm max}$ ) and  $-60^\circ$  at the epicardium ( $\theta_{\rm epi}^{\rm max}$ ) with respect to the horizontal basal plane (Z=0). It is also assumed that the fibers' inclination goes to zero at the left ventricle apex ( $Z_{\rm LV}^{\rm apex}$ ), so the expressions for the fiber angle on the myocardium boundaries read

$$\theta_{\text{epi}} = \theta_{\text{epi}}^{\text{max}} \left( 1 - \frac{Z}{Z_{\text{LV}}^{\text{apex}}} \right)$$

$$\theta_{\rm end} = \theta_{\rm end}^{\rm max} \left( 1 - \frac{Z}{Z_{\rm LV}^{\rm apex}} \right)$$

Across the cardiac walls the fiber angle varies linearly as

$$\theta = \beta \theta_{end} + (1 - \beta) \theta_{epi}$$

where  $\beta$  is a dimensionless parameter representing the fiber distance to the epicardium boundary. It takes values between 0 (epicardium) and 1 (endocardium), and it is an expression based on the fiber distance to the epicardium,  $D_{\rm epi}$ , and to the endocardium,  $D_{\rm end}$ ,

$$\beta = \frac{D_{\text{epi}}}{D_{\text{epi}} + D_{\text{end}}} \tag{1}$$

The myocardium is modeled as an anisotropic hyperelastic material with three preferential directions: fiber direction  $(\mathbf{a})$ , sheet direction  $(\mathbf{s})$  and normal to sheet direction  $(\mathbf{n})$ . This reference system can be approximated through a composition of coordinate systems.

The coordinate system used to define the material and electrical tissue properties is created in two steps. First, the transmural direction is obtained through the use of the Curvilinear **Coordinate** interface. It is assumed that the transmural direction coincides with the sheet direction  $(\mathbf{s})$ . The resulting curvilinear system has the first basis vector oriented in the sheet direction, and the second basis vector oriented towards the apico-basal direction (Figure 4).

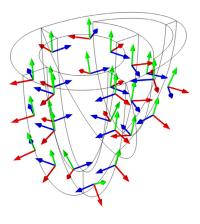




Figure 4: Intermediate coordinate system obtained with the Curvilinear Coordinate interface. The first basis vector (red) corresponds to the transmural direction. Note that the transmural direction coincides with the sheet direction in this example.

This intermediate coordinate system is rotated with an angle  $\theta$  around the first basis vector  $(\mathbf{s})$  to align the third axis along the fiber direction  $\mathbf{a}$ . The resulting fiber orientation is shown in Figure 5.

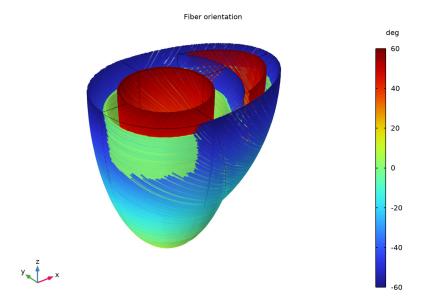


Figure 5: Fiber layout in the undeformed configuration. Note that the fiber angle changes along the transmural direction.

#### **ELECTROPHYSIOLOGY MODEL**

The electric potential  $\Phi$  in the myocardium is described by the following equation (Ref. 1)

$$\chi_{\rm m} C_{\rm m} \frac{\partial}{\partial t} V \Phi + \nabla \bullet (-D \nabla \Phi) + \chi_{\rm m} [I_{\rm ion}(\Phi, F, r_i)] = 0 \eqno(2)$$

where  $\chi_{\mathrm{m}}$  is the membrane surface to volume ratio,  $C_{\mathrm{m}}$  is the membrane capacitance, D is the conductivity tensor,  $I_{\text{ion}}$  is the ionic current per unit area, and F the deformation gradient. The ionic current depends on the potential, the deformation gradient, and other internal variables,  $r_i$ .

In this example, the ionic current is split into an excitation-induced, purely electrical part  $I_{\rm e}$ , and a stretch-induced part  $I_{\rm m}$ , as described in Ref. 2.

$$I_{\text{ion}}(\Phi, F, r_i) = I_{\text{e}}(\Phi, r_i) + I_{\text{m}}(F)$$
 (3)

The Aliev-Panfilov equations (Ref. 3) are used to represent the purely electrical part of the ionic current,  $I_e$ , as a function of the electric potential. These equations use one additional internal variable, and they are usually expressed in dimensionless form:

$$\tilde{I}_{e}(v,r) = c\phi(\phi - \alpha)(\phi - 1) + r\phi$$

$$\frac{\partial r}{\partial \tau} = \left(\gamma + \frac{\mu_1}{\mu_2 + \phi} r\right) [-r - c\phi(\phi - b - 1)]$$

Here,  $\phi$  is the dimensionless electric potential,  $\tau$  is the dimensionless time, and r is an internal variable called *recovery variable*. Furthermore, c,  $\alpha$ ,  $\gamma$ ,  $\mu_1$ ,  $\mu_2$ , and b are material parameters whose values are taken from Ref. 2 and can be found in Table 2.

TABLE 2: MATERIAL PARAMETERS FOR THE ALIEV-PANFILOV EQUATION.

PARAMETER	VALUE
c	8
α	0.01
γ	0.002
$\mu_1$	0.2
$\mu_2$	0.3
b	0.15

The a stretch-induced electric current  $I_{\mathrm{m}}$  is defined as

$$\tilde{I}_{\rm m}(F) = \theta G_s(\lambda(F) - 1)(\phi - \phi_s)$$

where  $\lambda$  is the stretch in the fiber direction,  $G_{\rm s}$  is the maximum conductance,  $\phi_{\rm s}$  is the resting electric potential for the ion channels, and  $\theta$  is an activation parameter. This expression assumes the value of 1 when the fibers are stretched, and 0 when they are compressed. The values of the additional parameters are taken from Ref. 2 and shown in Table 3.

TABLE 3: STRETCH-INDUCED CURRENT PARAMETERS.

PARAMETER	VALUE
$G_{ m s}$	10
$\phi_s$	0.6

A dimensional mapping of the ionic current equation (Equation 3) is used to match the experimental values of electric potential and activation time in the myocardium:

$$\Phi \,=\, \phi \beta_\phi + \delta_\phi$$

$$t = \beta_t \tau$$

Here,  $\beta_{\phi}$  and  $\delta_{\phi}$  are selected to match experimental values: the resting potential of the heart is -80 mV and the maximum potential value is 20 mV.

The time scaling parameter  $\beta_t$  is considered to be dependent on the activation time  $t_a$ , which shows better agreement with experimental observations (see Ref. 2 for details). During the cardiac cycle, the activation lapse (time between depolarization and repolarization) is not constant throughout the myocardium. Regions that are depolarized last are the first to repolarize. Therefore, the parameter  $\beta_t$  assumes the following expression

$$\beta_{\rm t} = (12.9 \text{ ms}) \left( 1 - \tau_0 \frac{t_{\rm a} - t_0}{t_1 - t_0} \right)$$
 (4)

where  $\tau_0$ ,  $t_0$ , and  $t_1$  are tuning parameters (Table 4).

TABLE 4: TIME MAPPING PARAMETERS

PARAMETER	VALUE
$\tau_0$	0.55
$t_0$	12[ms]
$t_1$	75[ms]

In this example, the activation time  $t_a$  depends on the Z coordinate and the vertical distance to the apex

$$t_{\rm a}(X, Y, Z) = (50 \,\mathrm{ms}) \left(1 - \frac{Z}{Z_{\rm LV}^{\rm apex}}\right)$$

The dimensional ionic current is then obtained from dimensionless purely electrical current  $I_{\rm e}(v,r)$ , and stretch-induced current  $I_{\rm m}(F)$ 

$$I_{\text{ion}} = C_{\text{m}} \frac{\beta_{\phi}}{\beta_{\text{t}}} (\tilde{I}_{\text{e}} + \tilde{I}_{\text{m}})$$

The conductivity tensor in Equation 2 is decomposed into an isotropic part and an anisotropic part, which depends on the fiber direction (Ref. 2)

$$D = (d_{iso}C_m\chi_{\mathrm{m}})I + (d_{ani}C_m\chi_{\mathrm{m}})\mathbf{a}_0 \otimes \mathbf{a}_0$$

where  $d_{iso} = 1 \text{ mm}^2/\text{ms}$  and  $d_{ani} = 0.1 \text{ mm}^2/\text{ms}$ .

#### **ACTIVE STRESS**

The active stress component, sa, is calculated by solving the following differential equation:

$$\frac{\partial s_{\mathbf{a}}}{\partial t} = \varepsilon(V)[k(\Phi - \Phi_{\mathbf{r}}) - s_{\mathbf{a}}] \tag{5}$$

where  $\varepsilon$  is a delay function introduced in Ref. 2:

$$\varepsilon(V) = \varepsilon_0 + (\varepsilon_0 - \varepsilon_1) \exp(-\exp(-\zeta(\Phi - \Phi_t)))$$

Here, k,  $\Phi_r$ ,  $\varepsilon_0$ ,  $\varepsilon_1$ ,  $\zeta$ , and  $\Phi_t$  are taken from Ref. 2 and shown in Table 5.

TABLE 5: ACTIVE STRESS PARAMETERS.

PARAMETER	VALUE
k	0.005[MPa/mV]
$\epsilon_0$	0.1[1/ms]
$\epsilon_1$	I[I/ms]
ζ	I[I/mV]
$\Phi_{ m r}$	-80[mV]
$\Phi_{ m t}$	0[mV]

The active stress obtained from Equation 5 is added to the second Piola–Kirchhoff stress in different percentages along the fiber, sheet and normal directions as described in Ref. 1:

$$S = S + s_{\mathbf{a}}(\mathbf{a}_0 \otimes \mathbf{a}_0) + 0.4s_{\mathbf{a}}(\mathbf{s}_0 \otimes \mathbf{s}_0) + 0.4s_{\mathbf{a}}(\mathbf{n}_0 \otimes \mathbf{n}_0)$$
 (6)

### MATERIAL MODEL

The cardiac tissue is considered to be hyperelastic, and the strain energy density is split into isotropic and anisotropic contributions

$$W = W_{iso} + W_{ani}$$

A compressible Neo-Hookean strain energy density is used for the isotropic part,

$$W_{\rm iso} = \frac{1}{2}\mu(I_1 - 3) + \mu {\rm log} J_{\rm el} + \frac{1}{2}\lambda {({\rm log} J_{\rm el})}^2$$

whereas the Holzapfel-Gasser-Ogden (HGO) model is used for the anisotropic contribution.

$$W_{\text{ani}} = \frac{k_1}{2k_2} (e^{k_2(\bar{I}_a - 1)^2} - 1) \tag{7}$$

Here,  $k_1$  and  $k_2$  are material properties, and  $ar{I}_a$  is the invariant of the isochoric Green-Cauchy strain tensor along the fiber direction:

$$\overline{I}_a = \overline{I}_a(\overline{C}_{el}, \mathbf{a}_0) = \mathbf{a}_0 \cdot \overline{C}_{el} \cdot \mathbf{a}_0$$
 (8)

The anisotropic hyperelastic parameters are given in Table 6.

TABLE 6: MATERIAL PROPERTIES.

Material properties	Value
λ (Ref. 2)	0.5[MPa]
μ (Ref. 2)	0.2[MPa]
k <sub>1</sub> (Ref. 1)	1.685[kPa]
k <sub>2</sub> (Ref. 1)	15.779

## **BOUNDARY AND INITIAL CONDITION**

The following conditions are applied to simulate the ventricle contractions:

- The displacement of the basal surface is constrained.
- Zero flux boundary conditions are used in the additional equations for  $\Phi$ , r, and  $s_{\rm a}$ .

• An initial pulse of electric potential (-10 mV) is applied on a rectangular area on the basal surface between the ventricles (Figure 6).

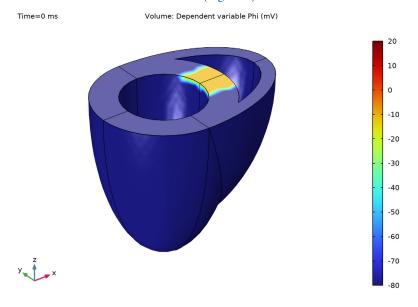


Figure 6: Initial impulse at the atrioventricular node.

## Results and Discussion

The model computes the contraction of the myocardium due to an electric stimulus. Figure 5 displays the fibers layout in the undeformed configuration.

Figure 7 shows the time variation of the electric potential distribution and the deformation of the cardiac walls. The depolarization of the cells produces an active stress that causes the myocardium to contract. There is an upward motion of the apex and a small torsion of the ventricles. The heart returns to its original state after 300 ms.

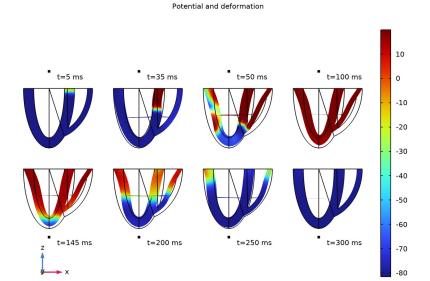


Figure 7: Depolarization and repolarization of the cardiac walls at different times during the cardiac cycle.

Figure 8 shows the activation potential at three different points. Note that the last cells to depolarize are the first one to repolarize. This effect is achieved by manipulating the dimensionless time constant as shown in Equation 4.

Figure 9 shows the internal volume variation of the left and right ventricles. Both chambers contract during the depolarization of the excited myocardial cells, thus reducing the internal volume. Then, the ventricles gradually return to their initial configuration to be again excited during the next heartbeat.

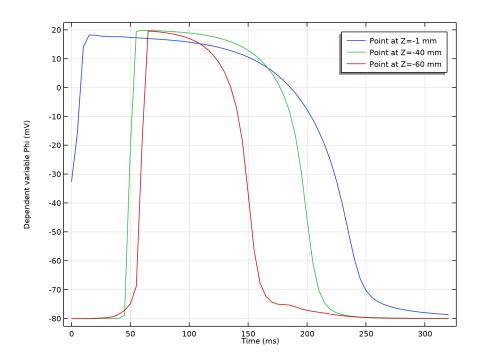


Figure 8: Plot of the activation duration at different locations.

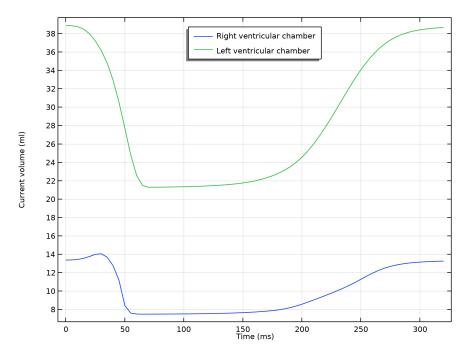


Figure 9: Volume variation of the left and right ventricular chambers.

# References

- 1. A.A. Bakir, A.A. Abed, M.C. Stevens, N.H. Lovell, and S. Dokos, "A Multiphysics Biventricular Cardiac Model: Simulations With a Left-Ventricular Assist Device," Front. Physiol., vol. 9, p. 1259, 2018.
- 2. S. Göktepe and E. Kuhl, "Electromechanics of the heart: a unified approach to the strongly coupled excitation-contraction problem," Comput. Mech., vol. 45, pp. 227–243, 2010.
- 3. M.P. Nash and A.V. Panfilov, "Electromechanical model of excitable tissue to study reentrant cardiac arrhytmias," Prog. Biophys. Mol. Biol., vol. 85,pp. 501-522, 2004.

The analysis is performed in two separated studies. In the first study the fiber orientation is computed. In a second study, the cardiac contraction following an electrical excitation is analyzed. In particular, the following steps are taken:

- The fibers paths are computed using the Wall Distance and Curvilinear Coordinate interfaces.
- The contribution of the electrophysiology model (PDE interfaces) is included in the Solid Mechanics interface through the **External Stress** feature.
- The **Fiber** feature is set up using the curvilinear fiber orientation.
- The fiber pattern is displayed for postprocessing.

The distances  $D_{\text{epi}}$  and  $D_{\text{endo}}$  used in Equation 1 to compute the dimensionless parameter  $\beta$  are determined by two **Wall Distance** interfaces. In one case the wall represents the endocardium, and in the other it represents the epicardium.

Inertial terms are neglected as reported in Ref. 2. The Structural Transient Behavior is set to Quasistatic in the Solid Mechanics interface setting.

The active stress (Equation 6) is added to the total stress with the **External Stress** feature. The fiber coordinate system is selected in the **Coordinate System Selection** section.

In the settings for the Fiber feature, select the appropriate Fiber Reference System as a reference coordinate system. Then, in the **Orientation** section, select the orientation of the fiber  $(\mathbf{a}_0)$  to be aligned with the **third axis**.

The **Fiber** feature automatically computes the corresponding invariants, for instance  $I_a$  as used in Equation 8, in order to compute the strain energy function  $W_{ani}$  as in Equation 7.

The option Stiffness in tension only is activated by default for the HGO model, and it evaluates the fibers' strain energy to zero if the fiber stretch is in compression. This means that the fibers contribute to tensile stresses only.

The model parameters taken from literature references already include the effect of the membrane surface to volume ratio,  $\chi_{\rm m}$ , and the membrane capacitance,  $C_{\rm m}$ . For this reason, these two parameters are set equal to 1 in this example.

The internal volume is computed through the use of Gauss's theorem to convert area integrals to volume integrals.

Application Library path: Nonlinear\_Structural\_Materials\_Module/ Hyperelasticity/biventricular\_cardiac\_model

## Modeling Instructions

From the File menu, choose New.

#### NEW

In the New window, click Model Wizard.

#### MODEL WIZARD

- I In the Model Wizard window, click **3D**.
- 2 In the Select Physics tree, select Mathematics>Wall Distance (wd).
- 3 Click Add.
- 4 Click Add.
- 5 In the Select Physics tree, select Mathematics>Curvilinear Coordinates (cc).
- 6 Click Add.
- 7 Click Study.
- 8 In the Select Study tree, select General Studies>Stationary.
- 9 Click M Done.

#### GEOMETRY I

- I In the Geometry toolbar, click Insert Sequence and choose Insert Sequence.
- **2** Browse to the model's Application Libraries folder and double-click the file biventricular cardiac model geom sequence.mph.
- 3 In the Geometry toolbar, click **Build All**.
- 4 Click the Go to Default View button in the Graphics toolbar. Full geometry instructions can be found in Appendix - Geometry Modeling Instructions.

#### **GLOBAL DEFINITIONS**

Heart Geometry Parameters

I In the Model Builder window, under Global Definitions click Parameters I.

2 In the Settings window for Parameters, type Heart Geometry Parameters in the Label text field.

#### DEFINITIONS

Create selections to identify the basal surface, the epicardium and the endocardium.

## Basal Surface

- I In the **Definitions** toolbar, click **\( \frac{1}{2} \) Explicit**.
- 2 In the Settings window for Explicit, type Basal Surface in the Label text field.
- 3 Locate the Input Entities section. From the Geometric entity level list, choose Boundary.
- 4 Click the Transparency button in the Graphics toolbar.
- **5** Select Boundaries 1, 3, 9, and 17 only.

#### LV-Endocardium

- I In the **Definitions** toolbar, click **\( \) Explicit**.
- 2 In the Settings window for Explicit, type LV-Endocardium in the Label text field.
- 3 Locate the Input Entities section. From the Geometric entity level list, choose Boundary.
- 4 Select Boundaries 6, 7, 12, and 16 only.

#### RV-Endocardium

- I In the **Definitions** toolbar, click **\( \bigcap\_{\bigcap} \) Explicit**.
- 2 In the Settings window for Explicit, type RV-Endocardium in the Label text field.
- 3 Locate the Input Entities section. From the Geometric entity level list, choose Boundary.
- 4 Select Boundaries 20 and 22 only.

## Ebicardium

- I In the **Definitions** toolbar, click **\( \) Explicit**.
- 2 In the Settings window for Explicit, type Epicardium in the Label text field.
- 3 Locate the Input Entities section. From the Geometric entity level list, choose Boundary.
- **4** Select Boundaries 4, 5, 10, 11, 15, 18, 19, and 21 only.

## Endocardium

- I In the **Definitions** toolbar, click **Union**.
- 2 In the Settings window for Union, type Endocardium in the Label text field.
- 3 Locate the Geometric Entity Level section. From the Level list, choose Boundary.
- **4** Locate the **Input Entities** section. Under **Selections to add**, click + **Add**.

- 5 In the Add dialog box, in the Selections to add list, choose LY-Endocardium and RY-Endocardium.
- 6 Click OK.

#### **GLOBAL DEFINITIONS**

## Structural Mechanics Parameters

- I In the Home toolbar, click Pi Parameters and choose Add>Parameters.
- 2 In the Settings window for Parameters, type Structural Mechanics Parameters in the Label text field.
- 3 Locate the Parameters section. Click Load from File.
- 4 Browse to the model's Application Libraries folder and double-click the file biventricular cardiac model mechanical passive param.txt.

#### Electrical Parameters

- I In the Home toolbar, click Pi Parameters and choose Add>Parameters.
- 2 In the Settings window for Parameters, type Electrical Parameters in the Label text field.
- 3 Locate the Parameters section. Click **Load from File.**
- **4** Browse to the model's Application Libraries folder and double-click the file biventricular cardiac model electrical param.txt.

### Active Stress Parameters

- I In the Home toolbar, click Pi Parameters and choose Add>Parameters.
- 2 In the Settings window for Parameters, type Active Stress Parameters in the Label text field.
- 3 Locate the Parameters section. Click **Load from File.**
- 4 Browse to the model's Application Libraries folder and double-click the file biventricular\_cardiac\_model\_active\_stress\_param.txt.

#### Conversion Factors Parameters

- I In the Home toolbar, click P Parameters and choose Add>Parameters.
- 2 In the Settings window for Parameters, type Conversion Factors Parameters in the Label text field.
- 3 Locate the Parameters section. Click **Load from File.**
- 4 Browse to the model's Application Libraries folder and double-click the file biventricular cardiac model conversion param.txt.

To compute the orientation of the fibers in any point in the myocardium it is necessary to know its distance from both the epicardium and the endocardium.

#### WALL DISTANCE: EPICARDIUM

- I In the Model Builder window, under Component I (compl) click Wall Distance (wd).
- 2 In the Settings window for Wall Distance, type Wall Distance: Epicardium in the Label text field.

#### Wall I

- I In the Physics toolbar, click **Boundaries** and choose Wall.
- 2 In the Settings window for Wall, locate the Boundary Selection section.
- 3 From the Selection list, choose Epicardium.

## WALL DISTANCE: ENDOCARDIUM

- I In the Model Builder window, under Component I (compl) click Wall Distance 2 (wd2).
- 2 In the Settings window for Wall Distance, type Wall Distance: Endocardium in the Label text field.
- 3 In the Physics toolbar, click **Boundaries** and choose Wall.

#### Wall I

- I In the Settings window for Wall, locate the Boundary Selection section.
- 2 From the Selection list, choose Endocardium.

Assuming that the sheets are oriented perpendicularly to the wall, their direction can be found by computing the transmural direction.

#### SHEET DIRECTION

- I In the Model Builder window, under Component I (compl) click Curvilinear Coordinates (cc).
- 2 In the Settings window for Curvilinear Coordinates, type Sheet Direction in the Label text field.
- 3 Locate the Settings section. Select the Create base vector system check box.

#### Coordinate System Settings 1

- I In the Model Builder window, under Component I (compl)>Sheet Direction (cc) click Coordinate System Settings 1.
- 2 In the Settings window for Coordinate System Settings, locate the Settings section.
- 3 From the Second basis vector list, choose z-axis.

Diffusion Method I

In the Physics toolbar, click **Domains** and choose **Diffusion Method**.

- I In the Physics toolbar, click 🖳 Attributes and choose Inlet.
- 2 In the Settings window for Inlet, locate the Boundary Selection section.
- 3 From the Selection list, choose Endocardium.

Diffusion Method I

In the Model Builder window, click Diffusion Method 1.

Outlet I

- I In the Physics toolbar, click 🖳 Attributes and choose Outlet.
- 2 In the Settings window for Outlet, locate the Boundary Selection section.
- 3 From the Selection list, choose Epicardium.

#### MESH I

- I In the Model Builder window, under Component I (compl) click Mesh I.
- 2 In the Settings window for Mesh, locate the Physics-Controlled Mesh section.
- **3** From the **Element size** list, choose **Finer**.
- 4 Click III Build All.

The first study is used to obtain the sheets' direction and the distance from the walls. These quantities can be used to find the fibers' direction.

#### STUDY: FIBER DIRECTION

- I In the Model Builder window, click Study I.
- 2 In the Settings window for Study, type Study: Fiber Direction in the Label text field.
- 3 In the Home toolbar, click **Compute**.

#### RESULTS

3D Plot Group 1, 3D Plot Group 2, Coordinate system (cc), Vector Field (cc)

- I In the Model Builder window, under Results, Ctrl-click to select 3D Plot Group I, 3D Plot Group 2, Vector Field (cc), and Coordinate system (cc).
- 2 Right-click and choose Group.

Study: Fiber Direction

In the Settings window for Group, type Study: Fiber Direction in the Label text field.

Add variables related to the fibers orientation.

#### DEFINITIONS

### Fiber Orientation

- I In the Model Builder window, expand the Component I (compl)>Definitions node.
- 2 Right-click **Definitions** and choose **Variables**.
- 3 In the Settings window for Variables, type Fiber Orientation in the Label text field.
- 4 Locate the Variables section. Click **Load from File.**
- **5** Browse to the model's Application Libraries folder and double-click the file biventricular cardiac model fibers.txt.

The fibers reference system is obtained by rotating the curvilinear coordinate system found in the previous study.

## Rotated System 2 (sys2)

- I In the Definitions toolbar, click Z Coordinate Systems and choose Rotated System.
- 2 In the Settings window for Rotated System, locate the Rotation section.
- 3 Find the Euler angles (Z-X-Z) subsection. In the  $\beta$  text field, type theta.

## Fiber Reference System

- I In the **Definitions** toolbar, click Z Coordinate Systems and choose Composite System.
- 2 In the Settings window for Composite System, type Fiber Reference System in the Label text field.
- 3 Locate the Input Systems section. From the Base system list, choose Curvilinear System (cc) (cc\_cs).
- 4 From the Relative system list, choose Rotated System 2 (sys2).

Create a cylindrical system for postprocessing purposes.

## Cylindrical System 4 (sys4)

- I In the Definitions toolbar, click  $\sqrt[2]{x}$  Coordinate Systems and choose Cylindrical System.
- 2 In the Settings window for Cylindrical System, locate the Coordinate Names section.
- 3 From the Frame list, choose Material (X. Y. Z).

Boundary System 1 (sys1), Curvilinear System (cc) (cc\_cs), Cylindrical System 4 (sys4), Fiber Reference System (sys3), Rotated System 2 (sys2)

- I In the Model Builder window, under Component I (compl)>Definitions, Ctrl-click to select Boundary System I (sys1), Curvilinear System (cc) (cc\_cs), Rotated System 2 (sys2), Fiber Reference System (sys3), and Cylindrical System 4 (sys4).
- 2 Right-click and choose **Group**.

## Coordinate Systems

- I In the Settings window for Group, type Coordinate Systems in the Label text field.
- 2 In the Model Builder window, collapse the Coordinate Systems node.

Now we have all information needed to simulate the contraction. Add a Solid Mechanics interface and three PDE interfaces. The three PDEs will be used to solve the monodomain equation and to compute the active stress.

## COMPONENT I (COMPI)

In the Home toolbar, click Windows and choose Add Physics.

#### ADD PHYSICS

- I Go to the Add Physics window.
- 2 In the tree, select Structural Mechanics>Solid Mechanics (solid).
- 3 Find the Physics interfaces in study subsection. In the table, clear the Solve check box for Study: Fiber Direction.
- 4 Click Add to Component I in the window toolbar.
- 5 In the tree, select Mathematics>PDE Interfaces>Coefficient Form PDE (c).
- 6 In the table, clear the Solve check box for Study: Fiber Direction.
- 7 Click Add to Component I in the window toolbar.
- 8 In the tree, select Mathematics>PDE Interfaces>Coefficient Form PDE (c).
- 9 In the table, clear the Solve check box for Study: Fiber Direction.
- **10** Click **Add to Component 1** in the window toolbar.
- II In the tree, select Mathematics>PDE Interfaces>Coefficient Form PDE (c).
- 12 In the table, clear the Solve check box for Study: Fiber Direction.
- 13 Click Add to Component 1 in the window toolbar.
- 14 In the tree, select Mathematics>PDE Interfaces>Coefficient Form PDE (c).
- 15 In the table, clear the Solve check box for Study: Fiber Direction.
- 16 In the Home toolbar, click and Physics to close the Add Physics window.

#### SOLID MECHANICS (SOLID)

- I In the Settings window for Solid Mechanics, locate the Structural Transient Behavior section.
- 2 From the list, choose Quasistatic.
- 3 Click to expand the Discretization section. From the Displacement field list, choose Linear.

Hyperelastic Material 1

- I Right-click Component I (compl)>Solid Mechanics (solid) and choose Material Models> Hyperelastic Material.
- 2 In the Settings window for Hyperelastic Material, locate the Domain Selection section.
- 3 From the Selection list, choose All domains.

Fiber 1

In the Physics toolbar, click 🕞 Attributes and choose Fiber.

#### MATERIALS

Material I (mat I)

- I In the Model Builder window, under Component I (compl) right-click Materials and choose Blank Material.
- 2 In the Settings window for Material, locate the Material Contents section.
- **3** In the table, enter the following settings:

Property	Variable	Value	Unit	Property group
Lamé parameter $\lambda$	lambLame	lambda_lame	N/m²	Lamé parameters
Lamé parameter $\mu$	muLame	mu_lame	N/m²	Lamé parameters
Density	rho	rhos	kg/m³	Basic
Fiber stiffness	kIHGO	af	Pa	Holzapfel-Gasser- Ogden
Model parameter	k2HGO	bf	I	Holzapfel-Gasser- Ogden
Fiber dispersion	k3HGO	0	I	Holzapfel-Gasser- Ogden

## ELECTROPHYSIOLOGY: TRANSMEMBRANE POTENTIAL (PHI)

I In the Model Builder window, under Component I (compl) click Coefficient Form PDE (c).

- 2 In the Settings window for Coefficient Form PDE, type Electrophysiology: Transmembrane Potential (Phi) in the Label text field.
- 3 Locate the Units section. Click Define Dependent Variable Unit.
- 4 In the Dependent variable quantity table, enter the following settings:

Dependent variable quantity	Unit
Custom unit	V

**5** In the **Source term quantity** table, enter the following settings:

Source term quantity	Unit
Custom unit	A/m^3

- **6** Click to expand the **Discretization** section. From the **Element order** list, choose **Linear**.
- 7 From the Frame list, choose Material.
- 8 Click to expand the Dependent Variables section. In the Field name text field, type Phi.
- **9** In the **Dependent variables** table, enter the following settings:

Phi

## ELECTROPHYSIOLOGY: CONDUCTANCE OF SLOW PROCESSES (R)

- I In the Model Builder window, under Component I (compl) click Coefficient Form PDE 2 (c2).
- 2 In the Settings window for Coefficient Form PDE, type Electrophysiology: Conductance of Slow Processes (r) in the Label text field.
- 3 Click to expand the Discretization section. Locate the Units section. In the Source term quantity table, enter the following settings:

Source term quantity	Unit
Custom unit	1/s

- 4 Locate the Discretization section. From the Element order list, choose Linear.
- 5 From the Frame list, choose Material.
- 6 Locate the Dependent Variables section. In the Field name text field, type r.
- 7 In the **Dependent variables** table, enter the following settings:

r

#### ACTIVE STRESS (SA)

- I In the Model Builder window, under Component I (compl) click Coefficient Form PDE 3 (c3).
- 2 In the Settings window for Coefficient Form PDE, type Active Stress (Sa) in the Label text field.
- 3 Locate the Units section. Click Define Dependent Variable Unit.
- 4 In the Dependent variable quantity table, enter the following settings:

Dependent variable quantity	Unit
Custom unit	N/m^2

5 In the Source term quantity table, enter the following settings:

Source term quantity	Unit
Custom unit	N/m^2/s

- 6 Locate the Discretization section. From the Element order list, choose Linear.
- 7 From the Frame list, choose Material.
- 8 Locate the Dependent Variables section. In the Field name text field, type Sa.
- **9** In the **Dependent variables** table, enter the following settings:

Sa

#### DEFINITIONS

Electrophysiology Variables

- I In the Model Builder window, under Component I (compl) right-click Definitions and choose Variables.
- 2 In the Settings window for Variables, type Electrophysiology Variables in the Label text field.
- 3 Locate the Variables section. Click **Load from File**.
- **4** Browse to the model's Application Libraries folder and double-click the file biventricular cardiac model electrophysiology.txt.

To compute the internal volume of the chamber during the contraction using Gauss' theorem we need to integrate over the internal boundaries.

Integration I (intobl)

I In the Definitions toolbar, click Nonlocal Couplings and choose Integration.

- 2 In the Settings window for Integration, type intLV in the Operator name text field.
- 3 Locate the Source Selection section. From the Geometric entity level list, choose Boundary.
- 4 From the Selection list, choose LV-Endocardium.

Integration 2 (intLV2)

- I Right-click Integration I (intop I) and choose Duplicate.
- 2 In the Settings window for Integration, type intRV in the Operator name text field.
- 3 Locate the Source Selection section. Click Clear Selection.
- 4 Select Boundaries 19–22 only.

Ventricular Internal Volume

- I In the Model Builder window, right-click Definitions and choose Variables.
- 2 In the Settings window for Variables, type Ventricular Internal Volume in the Label text field.
- **3** Locate the **Variables** section. In the table, enter the following settings:

Name	Expression	Unit	Description
volumeLV	intLV(-x*solid.nx)	m³	Left ventricle internal volume
volumeRV	<pre>intRV(-x*solid.nx)</pre>	m³	Right ventricle internal volume

Define the partial differential equations to solve in order to obtain the active stress.

## ELECTROPHYSIOLOGY: TRANSMEMBRANE POTENTIAL (PHI) (C)

Coefficient Form PDE I

- I In the Model Builder window, expand the Component I (compl)> Electrophysiology: Transmembrane Potential (Phi) (c) node, then click Coefficient Form PDE 1.
- 2 In the Settings window for Coefficient Form PDE, locate the Diffusion Coefficient section.
- **3** From the list, choose **Symmetric**.
- **4** In the *c* table, enter the following settings:

D_iso+DfibXX	DfibXY	DfibXZ
DfibXY	D_iso+DfibYY	DfibYZ
DfibXZ	DfibYZ	D_iso+DfibZZ

- **5** Locate the **Source Term** section. In the f text field, type -Chi\_m\*(Ie+Im).
- **6** Locate the **Damping or Mass Coefficient** section. In the  $d_a$  text field, type  $Chi_m^*Cm$ .

#### Initial Values 1

- I In the Model Builder window, click Initial Values I.
- 2 In the Settings window for Initial Values, locate the Initial Values section.
- 3 In the Phi text field, type Phir+70[mV]\*( $Z \sim 1e-4[mm]$ )\*(X < 31[mm])\*(X > 0[mm])\* (Y > -10[mm])\*(Y < 10[mm]).

## ELECTROPHYSIOLOGY: CONDUCTANCE OF SLOW PROCESSES (R) (C2)

#### Coefficient Form PDE I

- I In the Model Builder window, expand the Component I (compl)> Electrophysiology: Conductance of Slow Processes (r) (c2) node, then click Coefficient Form PDE I.
- 2 In the Settings window for Coefficient Form PDE, locate the Diffusion Coefficient section.
- **3** In the c text field, type 0.
- 4 Locate the Absorption Coefficient section. In the a text field, type (1/betat)\*(gamma+(mu1/(phi+mu2))\*c\*phi\*(phi-b-1)).
- 5 Locate the Source Term section. In the f text field, type (1/betat)\*(-gamma\*c\*phi\*)(phi-b-1)-mu1/(phi+mu2)\*r^2).

## ACTIVE STRESS (SA) (C3)

#### Coefficient Form PDE I

- I In the Model Builder window, expand the Component I (compl)>Active Stress (Sa) (c3) node, then click Coefficient Form PDE 1.
- 2 In the Settings window for Coefficient Form PDE, locate the Diffusion Coefficient section.
- **3** In the c text field, type 0.
- **4** Locate the **Absorption Coefficient** section. In the a text field, type eps delay.
- **5** Locate the **Source Term** section. In the f text field, type eps\_delay\*kT\*(Phi-Phir).

## SOLID MECHANICS (SOLID)

In the Model Builder window, expand the Component I (compl)>Solid Mechanics (solid) node.

#### Fiber 1

- I In the Model Builder window, expand the Component I (compl)>Solid Mechanics (solid)> Hyperelastic Material I node, then click Fiber I.
- 2 In the Settings window for Fiber, locate the Coordinate System Selection section.
- 3 From the Coordinate system list, choose Fiber Reference System (sys3).
- 4 Locate the Orientation section. From the a list, choose Third axis.

The coupling between the potential and the deformation is obtained through the active stress. The active stress is added as an external stress. Use the fiber coordinate system to easily input the components.

## Hyperelastic Material I

In the Model Builder window, click Hyperelastic Material 1.

#### External Stress 1

- I In the Physics toolbar, click 🕞 Attributes and choose External Stress.
- 2 In the Settings window for External Stress, locate the Coordinate System Selection section.
- 3 From the Coordinate system list, choose Fiber Reference System (sys3).
- 4 Locate the External Stress section. From the list, choose Diagonal.
- **5** In the  $S_{ext}$  table, enter the following settings:

vs*Sa	0	0
0	vn*Sa	0
0	0	vf*Sa

### Prescribed Displacement I

- In the Physics toolbar, click Boundaries and choose Prescribed Displacement.
- 2 In the Settings window for Prescribed Displacement, locate the Boundary Selection section.
- 3 From the Selection list, choose Basal Surface.
- 4 Locate the Prescribed Displacement section. Select the Prescribed in x direction check box.
- **5** Select the **Prescribed in y direction** check box.
- 6 Select the Prescribed in z direction check box.

### ADD STUDY

I In the Home toolbar, click Add Study to open the Add Study window.

- 2 Go to the Add Study window.
- **3** Find the **Physics interfaces in study** subsection. In the table, clear the **Solve** check boxes for Wall Distance: Epicardium (wd), Wall Distance: Endocardium (wd2), and Sheet Direction (cc).
- 4 Find the Studies subsection. In the Select Study tree, select General Studies> Time Dependent.
- 5 Click Add Study in the window toolbar.
- 6 In the Home toolbar, click Add Study to close the Add Study window.

#### STUDY: EXCITATION-CONTRACTION

- I In the Model Builder window, click Study 2.
- 2 In the Settings window for Study, type Study: Excitation-Contraction in the Label text field.

Set up the solver and initialize the solution to generate the Fiber default plot.

#### Steb 1: Time Dependent

- I In the Model Builder window, under Study: Excitation-Contraction click Step 1: Time Dependent.
- 2 In the Settings window for Time Dependent, locate the Study Settings section.
- 3 From the Time unit list, choose ms.
- 4 In the Output times text field, type range (0,5,320).
- 5 Click to expand the Values of Dependent Variables section. Find the Values of variables not solved for subsection. From the Settings list, choose User controlled.
- 6 From the Method list, choose Solution.
- 7 From the Study list, choose Study: Fiber Direction, Stationary.
- 8 In the Study toolbar, click  $\underset{=}{\overset{\cup}{\cup}}$  Get Initial Value.

#### RESULTS

Study: Excitation-Contraction/Solution 2 (sol2)

- I In the Model Builder window, expand the Results>Datasets node, then click Study: Excitation-Contraction/Solution 2 (sol2).
- 2 In the Settings window for Solution, locate the Solution section.
- 3 From the Frame list, choose Material (X, Y, Z).

Here the steps to obtain the model thumbnail are shown.

## 3D Plot Group 10

In the Home toolbar, click **Add Plot Group** and choose **3D Plot Group**.

## Hyperelastic Material I (solid)

- I In the Model Builder window, expand the Results>Fibers (solid) node, then click Hyperelastic Material I (solid).
- 2 In the Settings window for 3D Plot Group, click to expand the Title section.
- 3 In the **Title** text area, type Fiber orientation.
- 4 In the Hyperelastic Material I (solid) toolbar, click  **Plot**.

#### Endocardium

- I In the Model Builder window, expand the Hyperelastic Material I (solid) node, then click Fiber 1.
- 2 In the Settings window for Streamline, type Endocardium in the Label text field.
- 3 Locate the Streamline Positioning section. From the Positioning list, choose On selected boundaries.
- 4 From the Point distribution list, choose Mesh based.
- 5 In the Element refinement text field, type 2.
- **6** Locate the **Selection** section. Click to select the **Method Activate Selection** toggle button.
- **7** Select Boundaries 1–3, 8, 9, 13, 14, and 17 only.

#### Filter 1

Right-click **Endocardium** and choose **Filter**.

## Color Expression

- I In the Model Builder window, expand the Results>Fibers (solid)> Hyperelastic Material I (solid)>Endocardium node, then click Color Expression.
- 2 In the Settings window for Color Expression, locate the Expression section.
- 3 In the Expression text field, type theta.
- 4 In the **Unit** field, type deg.
- 5 Locate the Coloring and Style section. From the Color table list, choose Rainbow.
- **6** Click to expand the **Range** section. Select the **Manual color range** check box.
- 7 In the Minimum text field, type -60.
- **8** In the **Maximum** text field, type 60.

#### Filter 1

- I In the Model Builder window, click Filter I.
- 2 In the Settings window for Filter, locate the Element Selection section.
- 3 In the Logical expression for inclusion text field, type Beta>0.95.

### Myocardium

- I In the Model Builder window, right-click Endocardium and choose Duplicate.
- 2 In the Settings window for Streamline, type Myocardium in the Label text field.
- 3 Locate the Selection section. Click Clear Selection.
- **4** Select Boundaries 2, 8, 13, and 14 only.
- 5 Click to expand the Inherit Style section. From the Plot list, choose Endocardium.

#### Filter I

- I In the Model Builder window, expand the Myocardium node, then click Filter I.
- 2 In the Settings window for Filter, locate the Element Selection section.
- 3 In the Logical expression for inclusion text field, type (Beta>0.45)\*(Beta<0.55)\*(Z<cL/9).

#### Epicardium

- I In the Model Builder window, right-click Myocardium and choose Duplicate.
- 2 In the Settings window for Streamline, type Epicardium in the Label text field.
- 3 Locate the Selection section. Click Clear Selection.
- **4** Select Boundaries 2, 3, 5, 8–11, 13–15, 17, and 18 only.

#### Filter I

- I In the Model Builder window, expand the Epicardium node, then click Filter I.
- 2 In the Settings window for Filter, locate the Element Selection section.
- 3 In the Logical expression for inclusion text field, type Beta<0.05\*((sys4.phi>-100[deg])\*(sys4.phi<190[deg])\*(Z>-cL/3) || (Z<-cL/3)).
- 4 In the Hyperelastic Material I (solid) toolbar, click **1** Plot.
- 5 Click the | | Show Grid button in the Graphics toolbar.
- **6** Click the **Zoom Extents** button in the **Graphics** toolbar.
- 3D Plot Group 10, 3D Plot Group 7, 3D Plot Group 8, 3D Plot Group 9, Stress (solid)
- I In the Model Builder window, under Results, Ctrl-click to select Stress (solid),
  - 3D Plot Group 7, 3D Plot Group 8, 3D Plot Group 9, and 3D Plot Group 10.

Remove defaults plots that are not used.

2 Right-click and choose **Delete**.

Create a 3D plot to display the active potential distribution while the simulation runs.

#### Potential

- I In the Home toolbar, click **Add Plot Group** and choose **3D Plot Group**.
- 2 In the Settings window for 3D Plot Group, type Potential in the Label text field.
- 3 Locate the Data section. From the Dataset list, choose Study: Excitation-Contraction/ Solution 2 (sol2).

#### Volume 1

- I Right-click **Potential** and choose **Volume**.
- 2 In the Settings window for Volume, locate the Expression section.
- **3** In the **Expression** text field, type Phi.
- 4 From the Unit list, choose mV.
- 5 Click to expand the Range section. Select the Manual color range check box.
- 6 In the Minimum text field, type -80.
- 7 In the Maximum text field, type 20.

## Deformation I

- I Right-click Volume I and choose Deformation.
- 2 In the Settings window for Deformation, locate the Scale section.
- 3 Select the **Scale factor** check box.
- 4 In the associated text field, type 1.

### STUDY: EXCITATION-CONTRACTION

- I In the Model Builder window, click Study: Excitation-Contraction.
- 2 In the Settings window for Study, locate the Study Settings section.
- 3 Clear the Generate default plots check box.

#### Step 1: Time Dependent

- I In the Model Builder window, expand the Study: Excitation-Contraction node, then click Step 1: Time Dependent.
- 2 In the Settings window for Time Dependent, click to expand the Results While Solving section.
- **3** Select the **Plot** check box.
- 4 From the Plot group list, choose Potential.

5 In the Home toolbar, click **Compute**.

#### RESULTS

#### Contraction, Snapshots

- I In the Home toolbar, click Add Plot Group and choose 3D Plot Group.
- 2 In the Settings window for 3D Plot Group, type Contraction, Snapshots in the Label text field.
- 3 Locate the Data section. From the Dataset list, choose Study: Excitation-Contraction/ Solution 2 (sol2).
- 4 Click to expand the **Title** section. From the **Title type** list, choose **Manual**.
- 5 In the Title text area, type Potential and deformation.
- **6** Clear the **Parameter indicator** text field.
- 7 Click to expand the **Plot Array** section. Select the **Enable** check box.
- 8 From the Array shape list, choose Square.
- **9** From the Array plane list, choose xz.
- 10 Click the Co to XZ View button in the Graphics toolbar.

#### Slice 1

- I Right-click Contraction, Snapshots and choose Slice.
- 2 In the Settings window for Slice, locate the Data section.
- 3 From the Dataset list, choose Study: Excitation-Contraction/Solution 2 (sol2).
- 4 From the Time (ms) list, choose 5.
- **5** Locate the **Expression** section. In the **Expression** text field, type Phi.
- **6** From the **Unit** list, choose **mV**.
- 7 Locate the Plane Data section. From the Plane list, choose ZX-planes.
- 8 In the Planes text field, type 1.
- 9 Click to expand the Plot Array section. Select the Manual indexing check box.

### Deformation I

- I Right-click Slice I and choose Deformation.
- 2 In the Settings window for Deformation, locate the Scale section.
- 3 Select the Scale factor check box.
- 4 In the associated text field, type 1.
- 5 In the Contraction, Snapshots toolbar, click Plot.

#### Slice 2

- I In the Model Builder window, under Results>Contraction, Snapshots right-click Slice I and choose **Duplicate**.
- 2 In the **Settings** window for **Slice**, click to expand the **Title** section.
- **3** From the **Title type** list, choose **None**.
- 4 Locate the Plane Data section. From the Plane list, choose XY-planes.
- 5 In the Planes text field, type 1.
- 6 Locate the Coloring and Style section. Clear the Color legend check box.
- 7 Click to expand the Inherit Style section. From the Plot list, choose Slice 1.

#### Annotation I

- I In the Model Builder window, right-click Contraction, Snapshots and choose Annotation.
- 2 In the Settings window for Annotation, locate the Annotation section.
- 3 In the **Text** text field, type t=5 ms.
- 4 Locate the **Position** section. In the **Z** text field, type 20.
- 5 Click to expand the Plot Array section. Select the Manual indexing check box.

#### Annotation 1, Slice 1, Slice 2

- I In the Model Builder window, under Results>Contraction, Snapshots, Ctrl-click to select Slice I, Slice 2, and Annotation I.
- 2 Right-click and choose **Duplicate**.

#### Slice 3

- I In the **Settings** window for **Slice**, click to expand the **Title** section.
- **2** From the **Title type** list, choose **None**.
- 3 Locate the Coloring and Style section. Clear the Color legend check box.
- 4 Locate the Inherit Style section. From the Plot list, choose Slice 1.
- 5 Locate the Data section. From the Time (ms) list, choose 35.
- 6 Locate the Plot Array section. In the Column index text field, type 1.

#### Slice 4

- I In the Model Builder window, click Slice 4.
- 2 In the Settings window for Slice, locate the Data section.
- **3** From the **Time (ms)** list, choose **35**.
- 4 Locate the Plot Array section. In the Column index text field, type 1.

#### Annotation 2

- I In the Model Builder window, click Annotation 2.
- 2 In the Settings window for Annotation, locate the Annotation section.
- 3 In the **Text** text field, type t=35 ms.
- 4 Locate the Plot Array section. In the Column index text field, type 1.
- 5 In the Contraction, Snapshots toolbar, click Plot.
- 6 Click the Zoom Extents button in the Graphics toolbar.

#### Annotation 2, Slice 3, Slice 4

- I In the Model Builder window, under Results>Contraction, Snapshots, Ctrl-click to select Slice 3, Slice 4, and Annotation 2.
- 2 Right-click and choose **Duplicate**.

#### Slice 5

- I In the **Settings** window for **Slice**, locate the **Data** section.
- 2 From the Time (ms) list, choose 55.
- 3 Locate the Plot Array section. In the Column index text field, type 2.

#### Slice 6

- I In the Model Builder window, click Slice 6.
- 2 In the Settings window for Slice, locate the Data section.
- **3** From the **Time (ms)** list, choose **55**.
- 4 Locate the Plot Array section. In the Column index text field, type 2.

#### Annotation 3

- I In the Model Builder window, click Annotation 3.
- 2 In the Settings window for Annotation, locate the Annotation section.
- 3 In the **Text** text field, type t=50 ms.
- 4 Locate the Plot Array section. In the Column index text field, type 2.
- 5 In the Contraction, Snapshots toolbar, click Plot.
- 6 Click the Zoom Extents button in the Graphics toolbar.

## Annotation 3, Slice 5, Slice 6

- I In the Model Builder window, under Results>Contraction, Snapshots, Ctrl-click to select Slice 5, Slice 6, and Annotation 3.
- 2 Right-click and choose **Duplicate**.

#### Slice 7

- I In the **Settings** window for **Slice**, locate the **Data** section.
- **2** From the Time (ms) list, choose 100.
- 3 Locate the Plot Array section. In the Column index text field, type 3.

#### Slice 8

- I In the Model Builder window, click Slice 8.
- 2 In the Settings window for Slice, locate the Data section.
- 3 From the Time (ms) list, choose 100.
- 4 Locate the Plot Array section. In the Column index text field, type 3.

#### Annotation 4

- I In the Model Builder window, click Annotation 4.
- 2 In the Settings window for Annotation, locate the Annotation section.
- 3 In the **Text** text field, type t=100 ms.
- 4 Locate the Plot Array section. In the Column index text field, type 3.
- 5 In the Contraction, Snapshots toolbar, click Plot.
- **6** Click the **Zoom Extents** button in the **Graphics** toolbar.

## Annotation 4, Slice 7, Slice 8

- I In the Model Builder window, under Results>Contraction, Snapshots, Ctrl-click to select Slice 7, Slice 8, and Annotation 4.
- 2 Right-click and choose **Duplicate**.

#### Slice 9

- I In the Settings window for Slice, locate the Data section.
- **2** From the Time (ms) list, choose 145.
- 3 Click to expand the Plot Array section. In the Row index text field, type -1.
- 4 In the Column index text field, type 0.

#### Slice 10

- I In the Model Builder window, click Slice 10.
- 2 In the Settings window for Slice, locate the Data section.
- 3 From the Time (ms) list, choose 145.
- 4 Locate the Plot Array section. In the Row index text field, type -1.
- **5** In the **Column index** text field, type **0**.

#### Annotation 5

- I In the Model Builder window, click Annotation 5.
- 2 In the Settings window for Annotation, locate the Annotation section.
- 3 In the **Text** text field, type t=145 ms.
- **4** Locate the **Position** section. In the **Z** text field, type -80.
- 5 Click to expand the Plot Array section. In the Row index text field, type -1.
- 6 In the Column index text field, type 0.
- 7 In the Contraction, Snapshots toolbar, click Plot.
- 8 Click the Zoom Extents button in the Graphics toolbar.

## Annotation 5, Slice 10, Slice 9

- I In the Model Builder window, under Results>Contraction, Snapshots, Ctrl-click to select Slice 9, Slice 10, and Annotation 5.
- 2 Right-click and choose **Duplicate**.

#### Slice 11

- I In the **Settings** window for **Slice**, locate the **Data** section.
- **2** From the Time (ms) list, choose **200**.
- 3 Locate the Plot Array section. In the Column index text field, type 1.

#### Slice 12

- I In the Model Builder window, click Slice 12.
- 2 In the Settings window for Slice, locate the Data section.
- **3** From the **Time (ms)** list, choose **200**.
- 4 Locate the Plot Array section. In the Column index text field, type 1.

#### Annotation 6

- I In the Model Builder window, click Annotation 6.
- 2 In the Settings window for Annotation, locate the Annotation section.
- 3 In the **Text** text field, type t=200 ms.
- 4 Locate the Plot Array section. In the Column index text field, type 1.
- 5 In the Contraction, Snapshots toolbar, click Plot.
- 6 Click the Zoom Extents button in the Graphics toolbar.

Annotation 6, Slice 11, Slice 12

- I In the Model Builder window, under Results>Contraction, Snapshots, Ctrl-click to select Slice 11, Slice 12, and Annotation 6.
- 2 Right-click and choose **Duplicate**.

Annotation 7, Slice 13, Slice 14

- I In the Model Builder window, under Results>Contraction, Snapshots, Ctrl-click to select Slice 13, Slice 14, and Annotation 7.
- 2 In the Settings window for Slice, locate the Data section.
- **3** From the **Time (ms)** list, choose **250**.
- 4 Locate the **Plot Array** section. In the **Column index** text field, type 2.

#### Slice 14

- I In the Model Builder window, click Slice 14.
- 2 In the Settings window for Slice, locate the Data section.
- 3 From the Time (ms) list, choose 250.
- 4 Locate the **Plot Array** section. In the **Column index** text field, type 2.

#### Annotation 7

- I In the Model Builder window, click Annotation 7.
- 2 In the Settings window for Annotation, locate the Plot Array section.
- 3 In the Column index text field, type 2.
- 4 Locate the Annotation section. In the Text text field, type t=250 ms.
- 5 In the Contraction, Snapshots toolbar, click Plot.
- **6** Click the **Zoom Extents** button in the **Graphics** toolbar.

Annotation 7, Slice 13, Slice 14

- I In the Model Builder window, under Results>Contraction, Snapshots, Ctrl-click to select Slice 13, Slice 14, and Annotation 7.
- 2 Right-click and choose **Duplicate**.

#### Slice 15

- I In the **Settings** window for **Slice**, locate the **Data** section.
- 2 From the Time (ms) list, choose 300.
- 3 Locate the Plot Array section. In the Column index text field, type 3.

#### Slice 16

I In the Model Builder window, click Slice 16.

- 2 In the Settings window for Slice, locate the Data section.
- 3 From the Time (ms) list, choose 300.
- 4 Locate the Plot Array section. In the Column index text field, type 3.

#### Annotation 8

- I In the Model Builder window, click Annotation 8.
- 2 In the Settings window for Annotation, locate the Annotation section.
- 3 In the **Text** text field, type t=300 ms.
- 4 Locate the Plot Array section. In the Column index text field, type 3.

## Slice 2

Click the **Zoom Extents** button in the **Graphics** toolbar.

#### Contraction, Snapshots

- I Click the Transparency button in the Graphics toolbar.
- 2 Click the Orthographic Projection button in the Graphics toolbar.
- 3 In the Model Builder window, click Contraction, Snapshots.
- 4 In the Contraction, Snapshots toolbar, click Plot.

## Volume Change

- I In the Home toolbar, click **Add Plot Group** and choose ID Plot Group.
- 2 In the Settings window for ID Plot Group, type Volume Change in the Label text field.
- 3 Locate the Data section. From the Dataset list, choose Study: Excitation-Contraction/ Solution 2 (sol2).
- 4 Locate the Plot Settings section. Select the y-axis label check box.
- 5 Click to expand the **Title** section. From the **Title type** list, choose **None**.
- 6 Locate the Plot Settings section. In the y-axis label text field, type Current volume (ml).
- 7 Locate the Legend section. From the Position list, choose Upper middle.

#### Global I

- I Right-click Volume Change and choose Global.
- 2 In the Settings window for Global, locate the y-Axis Data section.

**3** In the table, enter the following settings:

Expression	Unit	Description
volumeRV	ml	Right ventricle internal volume
volumeLV	ml	Left ventricle internal volume

- 4 Click to expand the Legends section. From the Legends list, choose Manual.
- **5** In the table, enter the following settings:

Legends		
Right ventricular chamber		
Left ventricular chamber		

6 In the Volume Change toolbar, click Plot.

#### Point at Z=-1 mm

- I In the Results toolbar, click Cut Point 3D.
- 2 In the Settings window for Cut Point 3D, type Point at Z=-1mm in the Label text field.
- 3 Locate the Data section. From the Dataset list, choose Study: Excitation-Contraction/ Solution 2 (sol2).
- 4 Locate the **Point Data** section. In the **X** text field, type 25.
- **5** In the **Y** text field, type 0.
- 6 In the **Z** text field, type -1.

### Point at Z=-40mm

- I Right-click Point at Z=-Imm and choose Duplicate.
- 2 In the Settings window for Cut Point 3D, type Point at Z=-40mm in the Label text field.
- 3 Locate the Point Data section. In the X text field, type 20.
- **4** In the **Y** text field, type 0.
- 5 In the Z text field, type -40.

## Point at Z=-60mm

- I Right-click **Point at Z=-40mm** and choose **Duplicate**.
- 2 In the Settings window for Cut Point 3D, type Point at Z=-60mm in the Label text field.
- 3 Locate the Point Data section. In the X text field, type 0.
- 4 In the Y text field, type 0.
- 5 In the **Z** text field, type -60.

#### Activation Time

- I In the Results toolbar, click \( \subseteq \text{ID Plot Group.} \)
- 2 In the Settings window for ID Plot Group, type Activation Time in the Label text field.
- **3** Click to expand the **Title** section. From the **Title type** list, choose **None**.

## Point Graph 1

- I Right-click Activation Time and choose Point Graph.
- 2 In the Settings window for Point Graph, locate the Data section.
- 3 From the Dataset list, choose Point at Z=-Imm.
- 4 Locate the y-Axis Data section. In the Expression text field, type Phi.
- **5** From the **Unit** list, choose **mV**.
- **6** Click to expand the **Legends** section. Select the **Show legends** check box.
- 7 From the Legends list, choose Manual.
- **8** In the table, enter the following settings:

Legends			
Point	at	Z=-1	mm

## Point Graph 2

- I Right-click **Point Graph I** and choose **Duplicate**.
- 2 In the Settings window for Point Graph, locate the Data section.
- 3 From the Dataset list, choose Point at Z=-40mm.
- **4** Click to expand the **Title** section. From the **Title type** list, choose **None**.
- **5** Locate the **Legends** section. In the table, enter the following settings:

# Legends Point at Z=-40 mm

## Point Graph 3

- I Right-click Point Graph 2 and choose Duplicate.
- 2 In the Settings window for Point Graph, locate the Data section.
- 3 From the Dataset list, choose Point at Z=-60mm.
- **4** Locate the **Legends** section. In the table, enter the following settings:

Legend	ls			
Point	at	Z=-60	mm	

5 In the Activation Time toolbar, click Plot.

## Heart Deformation

- I In the Results toolbar, click Animation and choose Player. Create an animation to see the excitation path.
- 2 In the Settings window for Animation, type Heart Deformation in the Label text field.
- 3 Locate the Scene section. From the Subject list, choose Potential.
- 4 Locate the Frames section. In the Number of frames text field, type 50.
- **5** Click the **Zoom Extents** button in the **Graphics** toolbar.

# Appendix - Geometry Modeling Instructions

From the File menu, choose New.

#### NEW

In the New window, click Model Wizard.

#### MODEL WIZARD

- I In the Model Wizard window, click **3D**.
- 2 Click M Done.

#### **GLOBAL DEFINITIONS**

## Heart Geometry Parameters

- I In the Model Builder window, under Global Definitions click Parameters I.
- 2 In the Settings window for Parameters, type Heart Geometry Parameters in the Label text field.
- 3 Locate the Parameters section. Click **Load from File**.
- **4** Browse to the model's Application Libraries folder and double-click the file biventricular\_cardiac\_model\_geom\_param.txt.

#### GEOMETRY I

- I In the Model Builder window, under Component I (compl) click Geometry I.
- 2 In the Settings window for Geometry, locate the Units section.
- **3** From the **Length unit** list, choose **mm**.

## Ellipsoid: Left Ventricle

I In the Geometry toolbar, click  $\bigcirc$  More Primitives and choose Ellipsoid.

- 2 In the Settings window for Ellipsoid, type Ellipsoid: Left Ventricle in the Label text field.
- 3 Locate the Size and Shape section. In the a-semiaxis text field, type aL.
- 4 In the b-semiaxis text field, type bL.
- 5 In the c-semiaxis text field, type cL.
- **6** Click to expand the **Layers** section. In the table, enter the following settings:

Layer name	Thickness (mm)
Layer 1	tL

Ellipsoid: Right Ventricle

- I Right-click Ellipsoid: Left Ventricle and choose Duplicate.
- 2 In the Settings window for Ellipsoid, type Ellipsoid: Right Ventricle in the Label text field.
- 3 Locate the Size and Shape section. In the a-semiaxis text field, type aR.
- 4 In the b-semiaxis text field, type bR.
- 5 In the c-semiaxis text field, type cR.
- **6** Locate the **Layers** section. In the table, enter the following settings:

Layer name	Thickness (mm)
Layer 1	tR

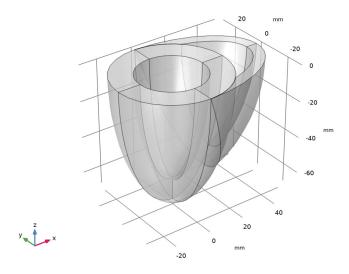
Partition Domains I (pard I)

- I In the Geometry toolbar, click Booleans and Partitions and choose **Partition Domains.**
- **2** Click the **Transparency** button in the **Graphics** toolbar.
- **3** On the object **elp2**, select Domains 1, 3, 5, 6, and 8 only.
- 4 In the Settings window for Partition Domains, locate the Partition Domains section.
- 5 From the Partition with list, choose Faces.
- 6 On the object elp1, select Boundaries 16 and 22 only.

Delete Entities I (dell)

- I In the Geometry toolbar, click Delete.
- 2 In the Settings window for Delete Entities, locate the Entities or Objects to Delete section.
- 3 From the Geometric entity level list, choose Domain.
- 4 On the object elp1, select Domains 2, 4, 5, 7, and 9 only.

- **5** On the object **pard1**, select Domains 1–7, 9, and 10 only.
- 6 Click **Build All Objects**.



## 7 Click **Build All Objects**.

Use virtual operations to ignore faces and edges to simplify the geometry and avoid unnecessary mesh refinement zones.

Ignore Faces I (igf1)

- I In the Geometry toolbar, click 🗠 Virtual Operations and choose Ignore Faces.
- 2 On the object fin, select Boundaries 11 and 20 only.

3 In the Geometry toolbar, click **Build All**.

